Design of Bio-molecular Feedback Systems

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Outline

- Part 1: Overview, history, and enabling technology
- Part 2: Simple modules fabricated: oscillators, toggles, and inverters
- Part 3: The challenge of composing modules together
- **<u>Part 4:</u>** Fabrication *in vivo* and *in vitro*

Part 1

Overview, history, and enabling technology

Why to Design Bio-molecular Feedback Systems?

MEDICAL APPLICATIONS

(e.g. targeted drug delivery)



ALTERNATIVE ENERGY

(e.g. bio-fuels) Making bacteria that...

- Produce hydrogen or ethanol



- Transform waste into energy

COMPUTING APPLICATIONS (e.g. molecular computing)

BIO-SENSING (e.g. detecting pathogens or toxins)

Synthetic Biology: A Historical Perspective

	Electronic Engineering	→			
<u>Electrical</u> Engineering	Vacuun	n Tube era	Transistor era		To Electronic computers
Ampere, 19 Coulomb, Faraday, Gauss, Henry, Kirchhoff Maxwell Ohm Fleming (a two-	onvented the diode terminal device)	19 Villiam Shockley explo bipolar junction trans December 1947, Bell L	48 The second se	196	54

(Nobel Prize in Physics in 1956)

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1964 Wildar at Fairchild Semiconductor

Synthetic Biology: A Historical Perspective



Key Enabling Technology



<u>Fluorescent Proteins</u>: allow through fluorescence microscopy to measure the concentration of a protein and thus the level of expression of the corresponding gene



Early modules fabricated in vivo



Part 2

Example modules

- Auto-repressed gene
- Toggle
- Loop oscillator
- Activator-repressor oscillator



For n=1:

Without negative feedbackWith negative feedback $x_1^{st} = \beta_1/\alpha$ $\frac{x_1(t)}{x_1^{st}} = 1 - e^{-\alpha t}$ $\frac{x_2(t)}{x_2^{st}} = \sqrt{1 - e^{-2\alpha t}},$ $\beta_2/\alpha \gg k$ $x_2^{st} = \sqrt{k\beta_2/\alpha}$

Negative feedback speeds up the response time (Rosenfeld et al 2002)









Loop oscillators: The repressilator





Elowitz and Leibler, Nature 2000





Loop oscillators: Design criteria

mRNA
$$\oint \frac{dr_{i}}{dt} = f_{1}(p_{n}) - \alpha_{1}r_{1}$$
protein
$$\oint \frac{dp_{1}}{dt} = r_{1} - \gamma_{1}p_{1}$$

$$\frac{dr_{i}}{dt} = f_{i}(p_{i-1}) - \alpha_{i}r_{i}$$

$$\frac{dp_{i}}{dt} = r_{i} - \gamma_{i}p_{i}$$

$$i = 2, 3, ..., n$$

$$f_{i}(p_{i-1}) = \frac{\beta_{i}p_{i-1}^{n}}{1 + p_{i-1}^{n}}$$

$$f_{i}(p_{i-1}) = \frac{\beta_{i}}{1 + p_{i-1}^{n}}$$

Circuits with same loop-gain are equivalent



Proof: Change of coordinates

$$r_{1}' = \frac{1}{\alpha_{1}} - r_{1}$$
 $r_{2}' = r_{2}$
 $p_{1}' = \frac{1}{\alpha_{1}\gamma_{1}} - p_{1}$ $p_{2}' = p_{2}$



Dynamical behavior of repressilators and promotilators

Invariant set and attractor

$$B(1,1,1) = [0,\frac{1}{\alpha_1}] \times [0,\frac{1}{\alpha_1\gamma_1}] \times [0,\frac{1}{\alpha_2}] \times [0,\frac{1}{\alpha_2\gamma_2}] \dots \times [0,\frac{1}{\alpha_n}] \times [0,\frac{1}{\alpha_n\gamma_n}]$$

is a positively invariant set and it contains a compact attractor for the dynamics.

Omega limit set

By Mallet-Paret and Smith Thorem (1990):

- Omega limit set is a single equilibrium, a single non-constant periodic orbit, or a structure consisting of a set of equilibria connected through homoclinic or heteroclinic orbits.
- Chaos can be ruled out.

Equilibria



Promotilators

Promotilators: Belong to the class of monotone dynamical systems (see Sontag 2005):

 $x(0) \le y(0) \implies \varphi(t, x(0)) \le \varphi(t, y(0))$

Theorem (M. Hirsh, 1988)

Let x(t) be the flow of an irreducible monotone system with the property that all forward orbits have compact closures. If the set of steady-states of the system is discrete, then the set of points x_0 for which $x(t, x_0)$ does not converge to a steady-state has Lebesgue measure zero.

Alternate stability, stability type derived by looking at 1D plot (Sontag, 2005)





Repressilators

- Repressilators have only one equilibrium.
- Instability of equilibrium Is sufficient for existence of periodic solution:

Theorem (Hastings et al. 1977) **Repressilators** $\dot{x}_1 = f_1(x_n, x_1)$ Let $x_{i} = f_{i}(x_{i-1}, x_{i})$ Let $\frac{\partial f_j}{\partial x_i} < 0, \frac{\partial f_j}{\partial x_{i-1}} > 0, \frac{\partial f_1}{\partial x} < 0, f_i(0,0) \ge 0, \frac{\partial f_1}{\partial x}$ be bounded from above Let $x^* = (x_1^*, x_2^*, \dots, x_n^*)$ be the steady steady-state such that $f_1(x_n, x_1) < 0$ when $x_n > x_n^*, x_1 > x_1^*$ and $f_1(x_n, x_1) > 0$ when $x_n < x_n^*, x_1 < x_1^*$ If Jacobian has eigenvalues with positive real part, then system has a nonconstant periodic orbit

Repressilators design

2

P₁ lac01

TetR

P₁ tet01

λ cl-lite

Lacl

- Can design oscillator by studying eigenvalues.
- Study robustness to parametric uncertainty
- Study tradeoffs

Symmetric design

$$\frac{dr_{1}}{dt} = f_{1}(p_{n}) - \delta r_{1} \qquad f_{i}(p) = \frac{\alpha^{2}}{1 + p^{n}}$$
$$\frac{dp_{1}}{dt} = r_{1} - \delta p_{1}$$
$$\frac{dr_{i}}{dt} = f_{i}(p_{i-1}) - \delta r_{i}$$
$$\frac{dp_{i}}{dt} = r_{i} - \delta p_{i}$$

Criterion employed in Elowitz & Liebler Nature 2000

Lacl, tetR, and lambdaCl all bind cooperatively to their target promoters: n~2

Symmetric design





Repressilators design



Asymmetric design



$$\frac{dr_1}{dt} = f_1(p_n) - \delta r_1$$

$$\frac{dp_1}{dt} = r_1 - \delta p_1$$

$$f_1(p) = \frac{\alpha_3^2}{1 + p^n}$$

$$\frac{dr_i}{dt} = f_i(p_{i-1}) - \delta r_i$$

$$f_{2,3}(p) = \frac{\alpha^2 p^n}{1 + p^n}$$

$$\frac{dp_i}{dt} = r_i - \delta p_i$$

Again: high cooperativity is a key for obtaining oscillations

Relaxation oscillators: Atkinson et al. clock

$$\frac{dr_A}{dt} = -\delta_1 r_A + F_1(A, B)$$

$$\frac{dA}{dt} = -\delta_A A + k_1 r_A$$

$$\frac{dr_B}{dt} = -\delta_2 r_B + F_2(A)$$

$$\frac{dB}{dt} = -\delta_B B + k_2 r_B,$$

$$F_1(A, B) = \frac{K_1 A^n + K_{A0}}{1 + \gamma_1 A^n + \gamma_2 B^m}$$

$$F_2(A) = \frac{K_2 A^n + K_{B0}}{1 + \gamma_3 A^n}$$
Combinatorial promoter:
Promoter with two inputs

ents)

50

B

В

2D Analysis and design

mRNA dynamics is 10 times faster than protein dynamics \rightarrow QSS approximation

$$\frac{dA}{dt} = -\delta_A A + f_1(A, B) \qquad f_1(A, B) = \frac{k_1}{\delta_1} F_1(A, B)$$
$$\frac{dB}{dt} = -\delta_B B + f_2(A), \qquad f_2(A) = \frac{k_2}{\delta_2} F_2(A)$$

The dynamics are bounded because the transcription functions are bounded.

There is one equilibrium point only if the nullclines intersect in one point only



Oscillator design requirements

By Poincarè-Bendixson theorem, since the system has one unstable equilibrium that is not a saddle and its trajectories are bounded in an invariant set, the omega-limit set is a periodic orbit



Promoter of the repressor must be tight (not leaky)

Promoter of the activator must be leaky

The promoter controlling the repressor B must be very strong Compared to that controlling the activator



Half life of the activator much smaller than the one of repressor (safe choice): can add degradation tags to the activator

Cooperativity of the activator at least 2

4D analysis and design



Bifurcation Analysis

$$\begin{split} \dot{r}_A &= -\delta_1/\epsilon \; r_A + F_1(A,B) \\ \dot{A} &= \nu(-\delta_A A + k_1/\epsilon \; r_A) \\ \dot{r}_B &= -\delta_2/\epsilon \; r_B + F_2(A) \\ \dot{B} &= -\delta_B B + k_2/\epsilon \; r_B, \end{split}$$





A robust Oscillator





Source of robustness: delay in the Negative feedback loops deriving From processes involved in the Formation of protein

Positive feedback loop: confers Robustness and tunability (the period can be tuned by changing the amounts Of inducers

Stricker et al. Nature 2008

Part 3

The challenge of composing modules together

- Retroactivity phenomenon and its modeling
- Insulation devices
- Implementation examples

Synthetic Biology: Enabling Technology for Biomolecular Circuit Design Ζ **Repressilator** Х P_Llac01 (Experimental Results) tetR-lite 60 140 450 λP_B 120 acl-lite 100 Fluorescence (arbitrary units) λ cl-lite Transcriptional component 60 P₁ tet01 Z 0 100 200 600 300 500 Time (min) (Elowitz and Leibler, Nature 2000) **Courtesy of Elowitz Lab** WORKING "MODULES" **NOT WORKING INTERCONNECTIONS** !

Modularity: A Fundamental Property



Internal circuitry of an OPAMP: It is composed of well defined modules



<u>Electronics and Control Systems Engineering</u> rely on modularity to predict the behavior of a complex network by the behavior of the composing subsystems.

Result: Computers, Videos, cell phones...



The Emergent integrated circuit of the cell [Hanahan & Weinberg (2000)]

Functional modules seem to recur also in <u>biological</u> <u>networks (e.g. Alon (2007))</u>. But...

But can they be interconnected and still maintain their behavior unchanged?

If not, what mechanism can be used to interconnect modules without altering their behavior?

Does nature already employ such mechanisms?



Courtesy of Ninfa Lab at Umich

How do we model these effects? How do we prevent them?

Outline

- A modeling framework for systems with retroactivity
- Retroactivity in transcriptional networks
- A lesson from OPAMPs: Insulation devices
- Design of a bio-molecular insulation device based on protease-feedback
- Fast time-scales as a key mechanism for insulation: phosphorylation
- Compromise between retroactivity attenuation and noise

A systems theory with retroactivity



A systems theory with retroactivity

<u>Def</u>: The I/O model of the **isolated system** is obtained when s=0 and when r is not an additional output

The interconnection of two systems is possible only when the internal state variable sets are disjoint:



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Gene regulatory circuitry: A network of transcriptional modules



But, is its input/output response unchanged upon interconnection?
Retroactivity in transcriptional networks has dramatic effects on the dynamics



Measure of the retroactivity

We seek to quantify the difference in the dynamics of the state X between the connected and isolated system

To compare the *X* dynamics we seek a 1D approximation for the connected system:

$$\frac{d\bar{X}}{dt} = k(t) - \delta\bar{X} + \bar{s}$$

Measure of retroactivity will be given by \overline{s}

Calculation of s

We exploit the time-scale separation between the output *X* dynamics and the dynamics of the input stage of the downstream component

$$\bar{s} = 0 \iff \frac{d\gamma(\bar{y})}{d\bar{y}} = 0 \implies$$
 we take $\frac{d\gamma(\bar{y})}{d\bar{y}}$ as a measure of retroactivity

Meaning and value of
$$\frac{d\gamma(\bar{y})}{d\bar{y}}$$

Isolated system dynamics:

$$\frac{dX}{dt} = f_I(X, t), \ f_I(X, t) = k(t) - \delta X$$

Approximate connected system dynamics:

$$\frac{dX}{dt} = f_C(X,t), \ f_C(X,t) = k(t) - \delta X - (k(t) - \delta X) \frac{d\gamma(y)}{dy}$$

$$\frac{d\gamma(y)}{dy} = \frac{|f_I(X,t) - f_C(X,t)|}{|f_I(X,t)|}$$

percentage difference between the isolated system dynamics and the approximate connected system dynamics

$$\frac{d\gamma(y)}{dy} = \frac{1}{1 + \frac{(1+X/k_d)^2}{p_{TOT}/k_d}} =: \mathcal{R}(X)$$

The value of the retroactivity measure for the interconnection through transcriptional regulation

Del Vecchio, Ninfa, and Sontag, Nature/EMBO-MSB 2008

Effect of R(X) on the dynamics



Does negative feedback always speeds up the response time? Retroactivity

$$\frac{dm_X}{dt} = u(t) - \delta_1 m_X$$
$$\frac{dX}{dt} = km_X - \delta_2 X,$$

$$\frac{dm_X}{dt} = k_1(p_{TOT} - C) - \delta_1 m_X$$

$$\frac{dX}{dt} = km_X - \delta_2 X - k_{on}(p_{TOT} - C)X + k_{off}C$$

$$\frac{dC}{dt} = k_{on}(p_{TOT} - C)X - k_{off}C.$$



Open loop system linearization matrix

 kk_1

$$F = \begin{bmatrix} -\delta_1 & 0\\ k & -\delta_2 \end{bmatrix} \qquad \bar{F} = \begin{bmatrix} -\delta_1 & -k_1 \frac{\bar{p}}{k_D + \bar{X}} \\ k & -\delta_2 \end{bmatrix} \Delta$$

$$\frac{kk_1}{\delta_2(\delta_1 - \delta_2)} < 1 \qquad \lambda_{MAX}(F) < \lambda_{MAX}(\bar{F}) \qquad \Delta = \operatorname{diag}\left(1, \frac{1}{1 + \bar{p}/(k_D + \bar{X})}\right)$$

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Dealing with retroactivity: Insulation devices

In general, we cannot <u>design</u> the downstream system (the load) such that it has low retroactivity. But, we can design an <u>insulation system</u> to be placed between the upstream and downstream systems.



1. The retroactivity to the input is approx zero: $r \approx 0$

2. The retroactivity to the output s is attenuated

3. The output is proportional to the input: y=c u

Reaching small retroactivity to the input r





 $R_i = \infty$ because the input stage of an OPAMP absorbs almost zero current



Choose the biochemical parameters of the input stage to allow a small value of $\mathcal{R}(Z)$

For example:

$$\mathcal{R}(Z) = rac{1}{1 + rac{(1 + Z/k_d)^2}{p_{TOT}/k_d}}$$

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Attenuation of the retroactivity to the output "s": Large feedback and large amplification

Non-inverting amplifier:



$$V_{out} = G(V_+ - V_-)$$

For G large enough:

$$V_{out} = \frac{V_+}{K}, \ K = \frac{R_1}{R_1 + R_2}$$

Conceptually:

$$y = G(u - Ky) + s \implies y = u \frac{G}{1 + KG} + \frac{s}{1 + KG}$$



Attenuation of the retroactivity to the output "s" in the transcriptional component

Connected system approximated dynamics

Isolated system

$$\frac{d\bar{X}}{dt} = (k(t) - \delta\bar{X})(1 - \frac{d\gamma(\bar{y})}{d\bar{y}}) \qquad \qquad \frac{dX}{dt} = k(t) - \delta X$$

Apply large input amplification G and large output feedback G'

$$\frac{d\bar{X}}{dt} = (Gk(t) - G'\bar{X} - \delta\bar{X})(1 - \frac{d\gamma(\bar{y})}{d\bar{y}}) \qquad \qquad \frac{dX}{dt} = Gk(t) - G'X - \delta X$$

Lemma. Consider the system

$$\frac{dX}{dt} = G(t)(u(t) - KX)$$

in which $G(t) \ge G_0 > 0$ and $|u'(t)| \le V$ uniformly in t. Then,
 $|X(t) - \frac{u(t)}{K}| \le \exp(-tG_0K)|X(0) - \frac{u(0)}{K}| + \frac{V}{G_0K^2}.$

Let G' = GK, then as G grows the signals $\overline{X}(t)$ and X(t) become close to each other

How do we realize a large input amplification and a large negative feedback?

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Simplified analysis: why should it attenuate "s"?

$$\frac{dZ}{dt} = k(t) - \delta Z + k_{-}Z_{bound} - k_{+}Z(p_{0,TOT} - Z_{bound})$$

$$\frac{dZ}{bound} = k_{+}Z(p_{0,TOT} - Z_{bound}) - k_{-}Z_{bound}$$

$$\frac{dT}{dt} = GZ_{bound} - \delta_{1}m_{X}$$
For a suitable signal $v(t)$
we have $m_{X} = Gv(t)$

$$\frac{dM_{X}}{dt} = GZ_{bound} - \delta_{1}m_{X}$$
Simplify to a one-step reaction model
$$\frac{dY}{dt} = -\eta_{1}YX + \beta W + \alpha G - \gamma Y + \eta_{2}W$$
and assuming Y at its equilibrium $\alpha G/\gamma$

$$\frac{dX}{dt} = -k_{on}C + k_{off}X(p_{TOT} - C),$$

$$\frac{dX}{dt} = \nu Gv(t) - \beta(\alpha G/\gamma)X - \delta_{2}X + k_{on}C - k_{off}X(p_{TOT} - C)$$

$$\frac{dX}{dt} = -k_{on}C + k_{off}X(p_{TOT} - C),$$

$$\frac{dX}{dt} = (\nu Gv(t) - (G' + \delta_{2})\overline{X})(1 - \frac{d\gamma(\overline{y})}{d\overline{y}}),$$
with $G' = KG$ and $K = \beta\alpha/\gamma$

As G and G' grow, $\overline{X}(t)$ becomes closer to X(t) generated by the isolated system

The input stage of the insulation device can be designed so as to have small "r"

$$\frac{dZ}{dt} = k(t) - \delta Z + k_{-}Z_{p} - k_{+}Z(p_{0,TOT} - Z_{p}) \longrightarrow r$$

$$\frac{dZ_{p}}{dt} = k_{+}Z(p_{0,TOT} - Z_{p}) - k_{-}Z_{p}$$

$$Applying singular perturbation we obtain the quasi steady state dynamics as$$

$$\frac{d\bar{Z}}{dt} = (k(t) - \delta\bar{Z})(1 - \mathcal{R}(\bar{Z})) \quad \mathcal{R}(\bar{Z}) = \frac{1}{1 + \frac{(1 + \bar{Z}/\bar{k}_d)^2}{p_{0,TOT}/\bar{k}_d}} \,\bar{k}_d = k_-/k_+$$

choose $p_{0,TOT}/\bar{k}_d \ll$ 1 to make $\mathcal{R}(\bar{Z})$ smaller

If $\bar{Z} \ll \bar{k}_d$, then the \bar{Z} to X relationship is about linear

Simulation results for the full system



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Fast time scales: A key mechanism for insulation

Basic Idea:



Claim: if G is large enough, signal x at the QSS is not affected by y.

Fast time scales: A key mechanism for insulation

Why would it work?

$$\frac{du}{dt} = f_0(t, u) + r(u, x)$$

$$\tilde{x} := x + y$$

$$\frac{dx}{dt} = Gf_1(u, x) + Gs(x, y)$$

$$\epsilon := 1/G$$

$$\frac{dy}{dt} = -Gs(x, y)$$

$$\frac{du}{dt} = f_0(t, u) + r(u, x)$$

$$\epsilon \frac{d\tilde{x}}{dt} = f_1(u, x)$$

$$\epsilon \frac{dy}{dt} = -s(x, y)$$
If the slow manifold is locally exponentially stable then $x = \gamma(u)$ with $f_1(u, \gamma(u)) = 0$

$$x(t) \text{ does not depend on y on the slow manifold}$$

A phosphorylation-based design for a biomolecular insulation device



Full system: The fast time-scale of the device is a key feature for attenuating "s"

Phosphorylation and dephosphorylation reactions are often much faster than protein production and decay:

$$\begin{split} \epsilon &= \delta/k_{off}, \ k_{on} = k_{off}/k_d, \ b_1 = \beta_1 X_{TOT} \epsilon/\delta, \\ a_1 &= \alpha_1 Y_{TOT} \epsilon/\delta, \ b_2 = \beta_2 \epsilon/\delta, \ a_2 = \alpha_2 \epsilon/\delta, \ c_i = \epsilon k_i/\delta \\ X_{TOT} \gg p_{TOT} & \text{When one sets } \epsilon = 0, \\ \frac{dz}{dt} &= k(t) - \delta(z - C_1) \\ \epsilon \frac{dC_1}{dt} &= -\delta(b_2 + c_1)C_1 + \delta b_1(z - C_1)(1 - \frac{X_p}{X_{TOT}} - \frac{C_1}{X_{TOT}} - \frac{C_2}{X_{TOT}}) \\ \epsilon \frac{dC_2}{dt} &= -\delta(c_2 + a_2)C_2 + \delta a_1 X_p(1 - \frac{C_2}{Y_{TOT}}) \\ \epsilon \frac{dX_p}{dt} &= \delta c_1C_1 + \delta a_2C_2 - \delta a_1 X_p(1 - \frac{C_2}{Y_{TOT}}) + \frac{\delta C - \delta/k_d(p_{TOT} - C)X_p}{V_{TOT}} \\ \epsilon \frac{dC}{dt} &= -\delta C + \delta/k_d(p_{TOT} - C)X_p \end{split}$$

Simulation results for the pho/depho insulation device



Xp for the isolated system Xp for the connected system

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High gains improve signal-to-noise ratio...



Courtesy of Elowitz lab (Caltech)

Bio-molecular processes are intrinsically stochastic

How do high gains (required for retroactivity attenuation) impact noise?



...but they also increase intrinsic noise at higher frequency



Jayanthi and Del Vecchio, CDC 2009

Part 4

Fabrication Technology

- Biobricks: overview
- In vitro transcriptional circuits

Parts, Devices, Systems

Devices

Parts

THE ABSTRACTION ADVANTAGE

Biological engineers can benefit from methods that made very large scale integrated (VLSI) electronics practical for the semiconductor industry. Standardization of technologies allowed chip engineers to specialize in circuit design or fabrication and to thereby manage complex problems at different levels of abstraction. Bio fab engineers can also cope with complexity by using abstraction hierarchies to hide unnecessary information. Thus, a bio fab designer working at

the level of whole systems need worry only about which devices to include and how to connect them to perform the desired function without having to manufacture each device from scratch. Similarly, a device-level designer should know the functions and compatibility of individual parts within a device, whereas a parts-level engineer should understand how each part works internally but need not be able to synthesize its DNA raw material.

Oscillator

ABSTRACTION HIERARCHY

Systems

Combinations of biological devices that perform functions encoded by humans. A system of three inverters, for example, can operate as an oscillator.

Devices

Combinations of parts that perform discrete tasks. One inverter can take an input signal—for example, "HIGH"—and convert it to the opposite output signal, "LOW." A common signal carrier standard, polymerase per second (PoPS), allows devices to more easily be combined into systems.

Parts

Genetic material encoding biological functions. A transcription operator such as part #R0051, for example, is a piece of DNA that works with a matching binding protein (#C0051 in this case) to regulate gene activity. Off-the-shelf parts with clear specifications can be combined in a variety of devices.

DNA Sequences for genetic parts. These can be specified by parts designers, manufactured off-site, then delivered. Fast synthesis technologies with low error rates make fabrication of custom DNA quick and reliable.

Part #: R0051

ORDER FORM

PoPS

Type: Transcription Operator Family: Protein:DNA Activity: 0-2 PoPS Requires: COOS1 **Gell Types: Enterobacteria** License: Public





David Baker, George Church, Jim Collins, Drew Endy, Joseph Jacobson, Jay Keasling, Paul Modrich, Christina Smolke and Ron Weiss Scientific American 2006

Library of standard Parts: Biobricks







Biobrick standard assembly



Any two biobricks can be combined in any order to form a new biobrick \rightarrow Modular assembly

In vivo Implementation



Plasmid: circular portion of DNA separate from the chromosomal DNA, which is capable of replicating independently of the chromosomal DNA



Transformation: process of inserting the plasmid within in the cell. It occurs by rendering the cells *competent,* (external membrane becomes permeable).

Inducers: signaling molecules that bind to repressors and disable them. The net effect is to start transcription. They can be added to the cell population to provide <u>input forcing</u> to the circuit

Reporter Genes: express proteins that produce an easily observable phenotype, for example, green fluorescent proteins, which causes cells to fluoresce green under blue Light. They are inserted after a gene of interest to measure its production rate. They Provide an easily <u>measurable output</u> to the system.



Example of a device: An inverter



Example of a device: A three-terminal device

Idea: design a BJT-like device



Bio-molecular implementation: using parts from lambda-switch and signal carrier: current/PoPS and voltage/protein concentration







P1 protease

Findings: Input/output PoPS gain in the linear region is 2

In vitro transcriptional circuits: circuits with no proteins



Transctiption is regulated with nucleic acids only (no proteins)


Implementing activation and repression

Switching transcription on and off by branch migration А R A' A' B This is the most favorable A and A' have more bases in common steady state energetic condition We can use this principle to turn ON and OFF the synthetic templates DNA template OFF Activator strand Fluorescent markers to monitor the Transcript n. dynamics of the switch R_n Template ON

Inhibitor strand

An in-vitro circuit: Rate regulator

- Idea: produce two chemicals at same rates
 - Common operation for metabolic networks maintain stoichiometry
 - Implemented using in vitro technology (test tubes instead of cells)



- Molecular programming for in vitro systems
 - Exploit Watson-Crick base pair binding (A-T, C-G)
 - Can "compile" functional specifications into RNA and DNA sequences
 - Circuits are biocompatible \Rightarrow some hope of embedding into cells

Franco, Winfree, and Murray, 52009

Comparing the two technologies

In vitro technology allows to run experiments in a fully controlled environment (the probe): Simulation data and experimental data usually agree

In vivo technology runs experiments in the cellular environment. Main challenges:

-<u>Cross talk</u>: the cell contains molecules that may interact with the circuit component
-<u>Noise</u>: the cellular environment is noisy and causes unpredictable stochastic fluctuations
-<u>Competition for shared resources</u>: the circuits that we introduce in the cell use cellular resources to work: ATC, RNAp, ribosomes, etc. They can thus severely impact the helthy behavior of the cell and as a consequence their own behavior



M Behar, HG Dohlman, and TC Elston. *PNAS 104(41):16146-51, 2007*

These are among the problems that make bio-molecular engineering *in vivo* fundamentally different from electrical engineering ⁷⁶



Summary

The ability of fabricating bio-molecular circuits has far reaching Applications: medical and energy are two examples





Stochasticity is an integral part of these systems and must be Explicitly considered for design